

INTERNATIONAL JOURNAL OF INNOVATIVE RESEARCH IN ELECTRICAL, ELECTRONICS, INSTRUMENTATION AND CONTROL ENGINEERING ol. 4. Issue 7. July 2016

Design of Low Complexity Adjustable Filter Bank for Personalized Hearing Aid Solutions

Pramela.B¹, Pratheeba.K² and Vanithalakshmi.M³

Department of Electronics and Communication Engineering, S.A. Engineering College, Chennai^{1, 2, 3}

Abstract: The auditory system is a very sensitive and complex network. Diseases, drugs, noise, trauma and aging may have resulted in varying degrees of hearing loss, which makes hearing impairments one of the most common sensory disturbances in the world. The most effective way to compensate hearing loss is to employ a hearing aid system which is an integration of voice amplification, noise reduction, feedback suppression, automatic program switching, environmental adaptation, and etc. The basic function of a hearing aid system is to amplify sounds selectively and then transfer the processed signal to the ear. The processed signal which is transferred to the ear enables the deaf people to hear the voice of the person who is near to them.

Keywords: Filter bank, Audiometer, ATMEL89S52 microcontroller, BAHA, Watch dog timers.

1. INTRODUCTION

Hearing is a complex process, so it should be no surprise In decompress section retrieve the given input voice but it that the causes of hearing loss are also complex. Hearing has less amplitude so we have to amplify the signal. After loss can occur because of damage to the ear, especially the amplification we use transducer for converting sound inner ear. For example, infants may be born with hearing signal into vibrating signal. loss caused by a viral infection that was acquired during pregnancy. Other times the cause is genetic and therefore due to changes in the genes involved in the hearing process. Sometimes, hearing loss is due to a combination • of genetic and environmental factors.

There is, for example, a genetic change that makes some people more likely to develop hearing loss after taking certain antibiotic medications. Understanding the genetic causes of deafness has important benefits. This knowledge not only allows doctors to inform families about their chances of having children with hearing loss, but it can also influence the way a person's deafness is treated. Whether a person's hearing loss is going to worsen can sometimes be predicted if the specific cause is known. Also, deafness may be only one of a group of medical problems that a person may have. For example, some people with hearing loss also have problems that affect other parts of the body, such as the heart, kidneys, or eyes. Knowing the genetic cause in these cases allows a doctor to predict the appearance of these other problems. It might seem reasonable to suspect a genetic cause of deafness only if the hearing loss runs in the family. But there are situations in which children have genetic deafness even though neither one of their parents are affected. This deafness can also be passed on to future generations. Genetic tests can therefore be helpful even if there is only one person in the family with hearing loss. In this proposed system we are going implement Signal-Processing Strategy for Restoration of Cross-Channel Suppression in Hearing-Impaired Listeners. It is very useful for hearing disability person. Voice input given to mike after that we use some filters to compress the voice. Cleared voice stored in storage device of controller, after processing of controller give another section depends upon • the channel selection.

2. EXISTING METHOD

- In the existing system, the bone anchored hearing aid (BAHA) is a surgically implanted device designed to provide a hearing aid to patients.
- The majority of the conventional hearing aid transmits sound through the medium of air conduction. BAHA stimulate the cochlea by transmitting the sound waves through the bones in our skull or bone conduction there by passing the outer and middle ear.



Figure1. BAHA Operated Image

3. PROPOSED SYSTEM

- In this project Signal-Processing Strategy for Restoration of Cross Channel Suppression is implemented in Hearing-Impaired Listeners.
- It is very useful for hearing disability person. The voice is given as the input.



INTERNATIONAL JOURNAL OF INNOVATIVE RESEARCH IN ELECTRICAL, ELECTRONICS, INSTRUMENTATION AND CONTROL ENGINEERING /ol. 4, Issue 7, July 2016

- information and by the compressor unit the voice is only RMS output. compressed for the clear signal which is get transferred to the WT voice IC where the data recording is • Voltage Regulator: possible.
- During the recording of data some amount of error signal will occur which is clear out by the decompression unit. Its efficiency is improved by amplification process.
- Then by using the transducer the sound signal is converted into the vibration signal. The vibration signal induces the auditory nerves and reaches the inner ear drum.

3.1 Advantages

- Reduces the size of the aid. •
- Suitable for different aged persons.
- It undergoes acceptable delay.
- It offers flexibility.

In this proposed system, the voice is given as the input, then for the future process and to remove some amount of ripples, here we are using some filter unit to separate the useful information and by the compressor unit the voice is compressed for the clear signal which is get transferred to the voice IC here the data recording is possible during the recording of data some amount of error signal will occur which is clear out by the decompression unit. Then by using the transducer the sound signal is converted into the vibration signal. The voice input is given to the transformer which converts one form of physical quantity into another. Then it enters into the voltage regulator and microcontroller. Microcontroller provides the highlyflexible and cost-effective solution to many embedded control applications.

3.2 Block Diagram of Hearing Aid



Figure2. Hearing Aid Block Diagram

• Transformer:

The potential transformer will step down the power supply (0-230V) to (0-6V) level. Then the secondary of voltage the potential transformer will be connected to the precision signal. Devices which perform an "Output" function are rectifier, which is constructed with the help of op-amp. generally called Actuators and are used to control some

Voltage regulators comprise a class of widely used ICs. Regulator IC units contain the circuitry for reference source, comparator amplifier, control device, and overload protection all in a single IC. IC units provide regulation of either a fixed positive voltage, a fixed negative voltage, or an adjustable set voltage. The regulators can be selected for operation with load currents from hundreds of milli amperes to tens of amperes, corresponding to power ratings from milli watts to tens of watts.

• ATMEL89S52 Microcontroller:

The AT89S52 is a low-power, high-performance CMOS microcontroller with bytes of 8-bit in-system programmable Flash memory. The device is manufactured Atmel's high-density nonvolatile using memory technology and is compatible with the industry-standard 80C51 instruction set and pin out. The on-chip Flash allows the program memory to be reprogrammed insystem or by a conventional non volatile memory programmer. By combining a versatile 8-bit CPU with insystem programmable Flash on a monolithic chip, the Atmel AT89S52 is a powerful microcontroller which provides a highly-flexible and cost-effective solution to many embedded control applications.



Figure3. ATMEL89S52 Microcontroller

• Sensor/Transducer:

The word "Transducer" is the collective term used for both Sensors which can be used to sense a wide range of different energy forms such as movement, electrical signals, radiant energy, thermal or magnetic energy etc., and Actuators which can be used to switch voltages or currents. There are many different types of Sensors and Transducers, both analog and digital and input and output available to choose from. The type of input or output transducer being used, really depends upon the type of signal or process being "Sensed" or "Controlled" but we can define a sensor and transducers as devices that converts one physical quantity into another. Devices which perform an "Input" function are commonly called Sensors because they "sense" a physical change in some characteristic that changes in response to some excitation, for example heat or force and covert that into an electrical The advantages of using precision rectifier are it will give external device, for example movement or sound.



INTERNATIONAL JOURNAL OF INNOVATIVE RESEARCH IN ELECTRICAL, ELECTRONICS, INSTRUMENTATION AND CONTROL ENGINEERING ol. 4, Issue 7, July 2016

Electrical Transducers are used to convert energy of one polarities attract, while like polarities (North and North, kind into energy of another kind, so for example, a South and South) repel. The internal configuration of a DC microphone (input device) converts sound waves into motor is designed to harness the magnetic interaction electrical signals for the amplifier to amplify (a process), between a current-carrying conductor and an external and a loudspeaker (output device) converts these electrical magnetic field to generate rotational motion. signals back into sound waves.



• Voice Board:

The APR9600 device offers true single-chip voice recording, non-volatile storage and playback capability for Every DC motor has six basic parts -- axle, rotor (a.k.a., 40 to 60 seconds. The device supports both random and sequential access of multiple messages. Sample rates are user-selectable, allowing designers to customize their design for unique quality and storage time needs. Integrated output amplifier, microphone amplifier, and AGC circuits greatly simplify system design. The device is ideal for use in portable voice recorders, toys, and many other consumer and industrial applications. APLUS integrated achieves these high levels of storage capability by using its proprietary analog/multilevel storage technology implemented in an advanced Flash nonvolatile memory process, where each memory cell can store 256 voltage levels. This technology enables the APR9600 device to reproduce voice signals in their natural form. It eliminates the need for encoding and compression, which often introduce distortion.



APR9600 Experimental board Figure 5. APR9600 Voice Board

In any electric motor, operation is based on simple A shunt-wound motor is a direct-current motor in which electromagnetism. A current-carrying conductor generates the field windings and the armature may be connected in a magnetic field when this is then placed in an external parallel across a constant-voltage supply. In adjustable magnetic field, it will experience a force proportional to speed applications, the field is connected across a the current in the conductor, and to the strength of the constant-voltage supply and the armature is connected external magnetic field. As you are well aware of from across an independent adjustable-voltage playing with magnets as a kid, opposite (North and South) Permanent magnet motors have similar control.



armature), stator, commutator, field magnet(s), and brushes. In most common DC motors (and all that Beamers will see), the external magnetic field is produced by high-strength permanent magnets. The stator is the stationary part of the motor; this includes the motor casing, as well as two or more permanent magnet pole pieces. The rotor (together with the axle and attached commutator) rotates with respect to the stator. The rotor consists of windings (generally on a core), the windings being electrically connected to the commutator. The above diagram shows a common motor layout -- with the rotor inside the stator (field) magnets. The geometry of the brushes, commutator contacts, and rotor windings are such that when power is applied, the polarities of the energized winding and the stator magnet(s) are misaligned, and the rotor will rotate until it is almost aligned with the stator's field magnets. As the rotor reaches alignment, the brushes move to the next commutator contacts, and energize the next winding.



Figure7. Circuit Diagram of Shunt Motor

supply.

IJIREEICE



INTERNATIONAL JOURNAL OF INNOVATIVE RESEARCH IN ELECTRICAL, ELECTRONICS, INSTRUMENTATION AND CONTROL ENGINEERING Vol. 4, Issue 7, July 2016



Figure8. Graphs for working of shunt motor

• Speaker

Speaker will control the electromagnetic wave into sound wave. It receives audio input from the device such as computer, audio receiver. This input may be either in analog or digital form. The sound produced by the speaker is defined by frequency and amplitude.



Figure9. Speaker

4. OUTPUT

The kit which involves the operation of the hearing aid is shown below. First the input voice is sensed by the sensor and it is then stored in the voice chip. This voice is processed and its efficiency is improved by the gamma tone filter which is in the voice IC.



Figure 5. Hearing Aid Kit

This processed voice then enters into the motor here the voice is converted into vibrations which can be audible by the person biting internal to their teeth. The supply required for this process is provided by the transformer which converts AC into DC (5V). This 5V supply is maintained constantly by the voltage regulator. The unwanted signals are removed by the filter which is placed next to the voltage regulator. This is overall working process of the hearing aid.

When the kit is recording the voice which is given as the input:



When the kit playbacks the voice which is recorded in the voice board and it is then heard by the deaf people:



5. CONCLUSION

A new strategy has been developed to reduce the complexity in filter bank for hearing aid solutions and to avoid the use of surgical operations. From these words the guilty of the deaf people while wearing this hearing aid is almost reduced. The complexity in the existing system is reduced to about 2.65 to 2.5 by using this method. It also reduces the irritation while hearing and to overcome the sound quality. This strategy is mainly used to reduce the complexity of the existing system by using filters. Hearing impairment has focused on very severe impairments, deafness and the hearing impairments of young people,



INTERNATIONAL JOURNAL OF INNOVATIVE RESEARCH IN ELECTRICAL, ELECTRONICS, INSTRUMENTATION AND CONTROL ENGINEERING Vol. 4, Issue 7, July 2016

rather than the moderate or partial hearing impairments that are common among elderly people. Most research on treatment for hearing impairment has focused on medical and surgical treatments rather than rehabilitative approaches.

REFERENCES

- [1] Aage R. Moller (2006), "Hearing: Anatomy, Physiology and Disorders of the Auditory System," Academic Press, 2nd edition.
- [2] Agnew. J (1998), "An overview of digital signal processing in hearing instruments," The Hearing Review.
- [3] Ahmad Kamarul, Ariff Bin Ibrahim (2007), "Biomedical engineering laboratory student pack", UTM johor.
- [4] Cassidy. R, J.O. Smith (2004), "A tunable, non sub sampled, non uniform filter bank for multi-band audition and level modification of audio signals," The 38th Asilomar Conference on Signals, Systems and Computers, vol.2, pp. 2228 - 2232.
- [5] Chong, K. S, B. H. Gwee, and J. S. Chang(2006), "A 16-channel low-power non uniform spaced filter bank core for digital hearing aid," IEEE Transaction on Circuits and Systems, vol. 53, no. 9, pp. 853–857.
- [6] Deng. T. B (2010), "Three-channel variable filter-bank for digital hearing aids" IET Signal Processing, vol. 4, no. 2, pp. 181-196.
- [7] Engebretson. A. M (1994), "Benefits of digital hearing aids," IEEE Engineering in Medicine and Biology Magazine, vol. 13, Issue 2, pp. 238-248.
- [8] Hamida. A. B (1999), "An adjustable filter-bank based algorithm for hearing aid systems," International Conference on Industrial Electronics, Control and Instrumentation, vol. 3, pp. 1187-1192.
- [9] Hermann, D, E. Chau, R.D. Dony and S.M. Areibi(2007), "Window Based Prototype Filter Design for Highly Oversampled Filter banks in Audio Applications," IEEE International Conference on Acoustics, Speech and Signal Processing, II-405 - II-408, 15-20, Honolulu, HI.
- [10] Hersh. M. A and M. A. Johnson et al., (2003) "Assistive Technology for the Hearing-Impaired, Deaf and Deaf-Blind," London, U.K.: Springer- Verlag.
- [11] Li. H, G. A. Jullien, V. S. Dimitrov, M. Ahmadi, and W. Miller(2002), "A 2-digit multidimensional logarithmic number system filter bank for a digital hearing aid architecture," IEEE Int. Symp. Circuits Syst., AZ, pp. II-760–763.
- [12] Lim. Y. C (1997), "A digital filter bank for digital audio systems," IEEE Transactions on Circuits and Systems, vol. 3, pp.848-849.
- [13] Mahesh. R and A. P. Vinod (2008), "Coefficient decimation approach for realizing reconfigurable finite impulse response filters," Proceedings of IEEE international symposium on circuits and systems, pp.81-84, Seattle USA.
- [14] Meng Tong Tan, J.S. Chang, and Yit Chow Tong (2001), "A novel low-voltage low-power wave digital filter bank for an intelligent noise reduction digital hearing instrument," IEEE International Symposium on Circuits and Systems, vol. 2, pp. 681 – 684, 06 -09, Sydney.
- [15] Noboru Ito and Tian-Liang Deng (2010), "Variable-Bandwidth Filter-Bank for Low-Power Hearing Aids," 3rd International Congress on Image and Signal Processing, pp.3207-3201.
- [16] Rong Dong, D. Hermann, R. Brennan, and E. Chau(2008), "Joint filter bank structures for integrating audio coding into hearing aid applications," IEEE International Conference on Acoustics, Speech and Signal Processing, pp. 1533 - 1536.
- [17] Slaney. M (1993), "An Efficient Implementation of the Patterson-Holds worth Auditory Filter bank," Technical Report 35, Apple Computer Co.,
- [18] Ying Wei and Debao Liu (2011), "A Design of Digital FIR Filter banks with Adjustable Sub band Distribution for Hearing Aids,"8th International Conference on Information, Communications and Signal Processing, pp.361-364, 13-16.
- [19] Ying Wei and Debao Liu (2013), "A Reconfigurable Digital Filter bank for Hearing Aid Systems with a Variety of Sound Wave Decomposition Plans", IEEE Transactions on Biomedical Engineering, Vol. 60, Issue: 6, pp. 1628 – 1635.
- [20] Yong Lian, and Ying Wei (2005), "A Computationally Efficient Non-Uniform FIR Digital Filter bank for Hearing Aid," IEEE

Transactions on Circuits and Systems I: Regular Papers, vol. 52, pp. 2754-2762.

[21] Yu-Ting Kuo, Tay-Jyi Lin, Yueh-Tai Li and Chih-Wei Liu(2010), "Design and Implementation of Low-Power ANSI S1.11 Filter bank for Digital Hearing Aids," IEEE Transactions on Circuits Systems: Regular Papers, Volume: 57, Issue: 7, pp.1684 –1696.